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Preclinical imaging of prostate cancer using radiolabeled antibodies

Susan Evans Axelsson



LUND

DOCTORAL DISSERTATION With permission of the Faculty of Medicine at Lund University, Sweden.

To be presented for public examination at the main lecture hall, Center for Molecular Pathology, JanWaldenströms gata 59, Skåne University Hospital Malmö for the degree of Doctor of Philosophy, Faculty of Medicine.

December 19, 2013 at 9:15 a.m.

Faculty opponent Professor Sten Nilsson, MD, PhD Karolinska Institute Department of Oncology-Pathology, Stockholm, Sweden

LUND UNIVERSITY	DOCTORAL DISSERTATION		
Department of Clinical Sciences, Malmö Division of Urological Cancers	Date of issue 19 th of December 2013		
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Author(s) Susan Evans Axelsson			
Title and subtitle Preclinical imaging of pro	ostate cancer using radiolabel	ed antibodies	
Target-specific molecular imaging with radiolable over the past 20 years, and is now an essential to and extent. Despite all efforts to detect and contro- men are still progressing to develop incurable met new methods based on target-specific imaging assessment and management of prostate cancer. The main purpose of this work was to investigate specific antigen (fPSA) and ICAM-1, as potential radiolabeled antibodies. The studies were desig targeting potential using animal models of prostat <i>in vivo</i> imaging modalities, <i>ex vivo</i> multi-radion measurements and immunohistochemistry were tuptake. In these studies, we found that radiolabeled Ku70/Ku80 antigen in prostate cancer xenografi labeled antibody. We also demonstrate that two a can efficiently target PSA positive prostate cancer animal models immune deficiency status can affe that ¹¹¹ In-R6.5 mAb outperformed the ¹⁷⁷ Lu-R6 complement to clinically used metabolic and proli Our <i>ex vivo</i> and <i>in vivo</i> investigations presented further studies of the Ku70/Ku80, fPSA and IC/ therapeutic applications based on dosimetry calcul	bol to provide information co of prostate cancer at an early castatic disease. Because of the is becoming increasingly three target antigens: Ku70/J candidates for imaging of prined to assess the <i>in vivo</i> a te cancer. Preclinical SPECT uclide digital autoradiograph used to obtain biokinetics and INCA-X mAb could effit ts in mice that first receive untibodies specific for fPSA (xenografts. In that study, we exist the antibody performance .5 or control IgG mAb and ferative probes. in this dissertation should AM-1 antigens. Future study	on disease presence stage, a number of is, development of important in the Ku80, free prostate ostate cancer using nd <i>ex vivo</i> tumor //CT and PET//CT ny, <i>ex vivo</i> activity nd specific activity ciently target the a predose of non- PSA30 and 5A10) also show that the e. Lastly, we show I can be used as a act as support for lies should include	
Key words: Prostate cancer, antibody imaging, Ku ICAM-1, R6.5, multi-nuclide imaging,	70/Ku80, INCA-X, free PSA preclinical SPECT/CT, prec	A, PSA30, 5A10, linical PET/CT	
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Preclinical imaging of prostate cancer using radiolabeled antibodies

Susan Evans Axelsson



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To David.

List of Papers

This dissertation is based on the following papers, which will be referred to in the text by their Roman numerals. The papers are appended at the end of the dissertation.

I. **Susan Evans Axelsson**, Oskar Vilhelmsson Timmermand, Charlotte Welinder, Carl Borrebaeck, Sven-Erik Strand, Thuy A. Tran, Bo Jansson* and Anders Bjartell*

Preclinical 111In-INCA-X monoclonal antibody imaging of Ku70/Ku80 antigen in prostate cancer.

Submitted for publication

II. **Susan Evans-Axelsson**, David Ulmert, Anders Örbom, Pernilla Peterson, Olle Nilsson, Johan Wennerberg, Joanna Strand, Karin Wingårdh, Tomas Olsson, Zandra Hagman, Vladimir Tolmachev, Anders Bjartell, Hans Lilja and Sven-Erik Strand

Targeting free prostate-specific antigen for in vivo imaging of prostate cancer using a monoclonal antibody specific for unique epitopes accessible on free prostate-specific antigen alone.

Cancer Biother Radiopharm. 2012 May;27(4):243-51.

III. Oskar Vilhelmsson Timmermand, **Susan Evans Axelsson**, Daniel J. Thorek, Anders Bjartell, Hans Lilja, Sven-Erik Strand, Thuy A. Tran* and David Ulmert*

Immunological and labeling strategy effects on free-PSA targeting antibody 5A10. *Manuscript*

IV. Anders Örbom^{*}, **Susan Evans Axelsson**^{*}, Bo Jansson, Oskar Vilhelmsson Timmermand, Thuy A. Tran, Anders Bjartell, Sven-Erik Strand

Intratumoral distribution and pharmacokinetics of the radiolabeled ICAM-1 targeting monoclonal antibody, R6.5 in a prostate cancer mouse model *Manuscript*

*Authors contributed equally to this work

Publications not included in the dissertation

Barbara Wegiel, **Susan Evans**, Rebecka Hellsten, L.E. Otterbein, Anders Bjartell, J.L. Persson Molecular Pathways in the Progression of Hormone-Independent and Metastatic Prostate Cancer *Current Cancer Drug Targets*. 2010; 10(4):392-401

Susan Evans, Nishtman Dizeyi, Per-Anders Abrahamsson, Jenny Persson The effects of a noval botanical agent TBS-101 on invasive prostate cancer in animal models *Anticancer research. 2009; 29(10):3917-3924*

Abbreviations

%IA/g	Percent of injected activity per gram
¹⁸ F-FCH	[18F]fluorocholine
¹⁸ F-FDG	2-[18F]fluoro-2-deoxy-D-glucose
¹¹¹ In	Indium-111
¹⁷⁷ Lu	Lutetium-177
⁸⁹ Zr	Zirconium-89
ADC	Antibody drug conjugates
AP	Anterior prostate (mouse)
BPH	Benign prostatic hypertrophy
CAD	Computer-assisted diagnosis software
CBRs	Complementary determining region
CHX-A"-DTPA	[(R)-2-Amino-3-(4-isothiocyanatophenyl)propy1]- <i>trans</i> -
	(S,S)-cyclohexane-1,2-diamine-pentaacetic acid
cPSA	Complexed PSA
CRPC	Castration resistant prostate cancer
СТ	Computed tomography
CTCs	Circulating tumor cells
CZ	Central zone
DARG	Digital autoradiography
DLP	Dorsal lateral prostate (mouse)
DOTA	1,4,7,10-tetraazacyclododecane-N,N',N",N"-tetraacetic acid
DP	Dorsal prostate (mouse)
FDA	The U.S. Food and Drug Administration
fPSA	Free prostate specific antigen
hK2	Human kallikrein 2
ICAM-1	Intercellular adhesion molecule-1
Ig	Immunoglobulin
IHC	Immunohistochemistry
IL-1	Cytokines like interleukin-1
ITLC	Instant thin layer chromatography
ISOBM	Oncodevelopmental Biology and Medicine
LP	Lateral prostate (mouse)
mAb	Monoclonal antibody

MRI	Magnetic Resonance Imaging
NMRI	Naval Medical Research Institute
PET	Position emission tomography
p.i.	Post-injection
PSCA	Prostate stem cell antigen
PSA	Prostate-specific antigen
PSMA	Prostate specific membrane antigen
PZ	Peripheral zone (human)
SPECT	Single-photon emission computed tomography
$T_{\frac{1}{2}}$	Half-life
TNF-alpha	Tumor necrosis factor alpha
tPSA	Total PSA
TZ	Transition zone (human)
USPSTF	U.S. Preventive Services Task Force
VP	Ventral prostate (mouse)

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Part I: The Prostate

A small leak can sink a great ship ~ Benjamin Franklin

The human prostate

The human prostate, though small, can become troublesome with age. The normal human prostate is a small exocrine gland that weighs between 18 and 30 g and is located directly below the bladder and surrounding the upper part of the urethra in males [1]. It is an accessory sex gland that secretes about 30 percent of the fluid that makes up semen and a common source of urological problems in men over the age of 40. Structurally, the human prostate is a walnut-shaped lobe divided into three major zones (Figure 1): the peripheral zone (PZ), the central zone (CZ) and the transition zone (TZ) [2].

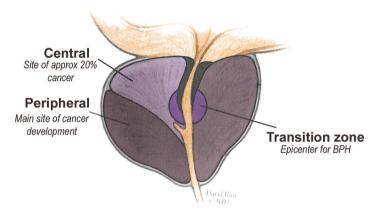


Figure 1. Schematic illustration of the anatomy of a human prostate. Adapted from Walsh et al. 2012 [1].

The PZ makes up the largest proportion of the prostate (70%) and is the site where the majority of prostate cancer originates. The TZ, surrounding the urethra, is the smallest zone of the normal prostate (5%) and is the epicenter for benign prostatic hyperplasia (BPH) development. The CZ surrounds the ejaculatory ducts making up about 25 percent of the prostate and accounting for the location of roughly 20 percent of prostate cancer development.

Microscopically, the prostate consists of glandular epithelial cells and smooth muscle stromal cells divided by a thin basement membrane. The prostate epithelium consists of three different cell types: secretory luminal cells, basal epithelial cells and neuroendocrine cells. The stroma serves as the structural support for the prostate and consists of extracellular matrix along with smooth muscle cells and fibroblast [1]. Normal stromal cells are heavily influenced by androgens and thus generate several paracrine/growth factors that direct the development, maintenance

and differentiation of the nearby epithelial cells [3]. It is in response to paracrine signaling from the stroma that normal luminal cells secrete prostatic fluids like prostate specific antigen (PSA) and acid phosphatase into the lumen of the gland to be released outside the body via the urethra [1].

The mouse prostate

Human and mouse prostates are significantly different, yet still similar enough to make the mouse a valuable model for prostate cancer research. Unlike the human prostate that is alobular, the mouse prostate is comprised of four lobes with distinctive histologic appearance and branching patterns (Figure 2): the anterior (AP)/coagulating gland, ventral (VP), dorsal (DP) and lateral (LP) prostate, located at the base of the bladder and incompletely surrounding the urethra.

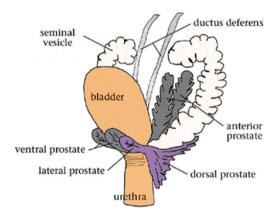


Figure 2. Schematic illustration of the anatomy of an adult mouse prostate. Adapted from Sugimura et al. 1986 [7].

Often the DP and LP are collectively referred to as the dorsolateral (DLP) lobe and it is in this lobe that the mouse prostate shares the most molecular and histological similarities to the PZ of the human prostate [1, 4, 5]. The human and mouse prostate both have similar secretory luminal, basal and neuroendocrine epithelial cell types and are composed of glands and ducts [6, 7]. However, in the human prostate, there is a true bilayer stratification between the basal cells and luminal cells whereas in the mouse prostate they are in direct contact with each other. Another difference to note is the amount of stroma in the prostates, whereas the proportion of stroma is much larger in the human prostate than in the mouse [6]. And unlike in the human, the mouse prostate is not prone to spontaneously develop pathological disorders.

Human prostatic non-cancer disorders

Prostatitis and BPH are two prostate disorders common to aging men that can mimic cancer, yet are not [8]. Prostatitis is a painful inflammation of the prostate and a common cause of urinary tract infection in men. If triggered by a bacterial infection (*acute and chronic bacterial prostatitis*), it can be treated with antibiotics. However, if it falls into the more common categories of *chronic prostatitis/chronic pelvic pain syndrome* or *asymptomatic inflammatory prostatitis*, then it is much harder to treat because antibiotics are ineffective and the precise cause is unknown. In these cases, doctors resort to treating the symptoms instead of directly treating the problem [8]. It has long been assumed that prostatitis is not a precursor to cancer forming. Nevertheless, more resent studies have suggested that inflammation could possibly be sufficient enough to develop cancer, although more research is needed before any firm conclusion can be formed [9, 10].

BPH is an enlargement of the prostate originating in the TZ and growing inwards eventually obstructing the urethra and thus interfering with urination [11, 12]. BPH is not life threatening and can be treated with medication or surgery.

Prostate cancer: indolent, insignificant or significant

A diagnosis of prostate cancer is not necessarily life threatening. A man with indolent prostate cancer will not have clinical symptoms and will not die from the disease [13]. And a man with a low Gleason score (≤ 6)¹, small tumor volume (<0.5cm³) and organ-confined prostate cancer will be diagnosed with clinically insignificant prostate cancer unlikely to progress to clinically significant cancer [14]. Prostate cancer is generally asymptomatic and often curable if detected in an early stage while still confined to the prostate.

Improved early detection methods and more personalized therapies for prostate cancer patients have helped to reduce the mortality rate in a number of developed countries, like the United States, Canada, France and Switzerland; yet this trend has not been seen to the same extent in other countries, like Denmark, Sweden and Italy [15, 16]. The differences are possibly due to the extent of which the early detection

¹ Gleason score – a histopathological grading system used by pathologist as a commonly used way to classify prostate cancer based on how it looks under a microscope.

methods, like measuring serum PSA concentrations and biopsy, are used. However, the improved screening methods have also lead to over-detecting and over-treating of prostate cancer that ultimately poses little or no risk to life and health. And thus, given that prostate cancer has a natural history of 10-20 years, there is a clear need to distinguish between aggressive and clinically insignificant cancer at an early stage.

Part II: Imaging Prostate Cancer

Simply generating an image, for which the implications to the patient are not understood, does not confer benefits to the patient.

FDA Guidance for Industry: Developing Medical Imaging Drug and Biological Products, 2004

Molecular imaging

Despite doctors' best efforts to detect and control prostate cancer at an early stage, a number of men are still progressing to develop metastatic disease. Molecular imaging is "the visualization, characterization and measurement of biological processes at the molecular and cellular levels in humans and other living systems [17]". Non-invasive *in vivo* imaging methods, such as single photon emission computed tomography (SPECT) and positron emission tomography (PET), allow physicians to get a wholebody picture of biological processes using targeted and disease specific radiolabeled probes. Because of this, target specific imaging is becoming increasingly important in the assessment and management of prostate cancer.

Current imaging tools available for preclinical and clinical use can be employed to:

- 1) visualize and stage local and metastatic disease
- 2) give a quantitative assessment of molecular targets to help guide treatment selection by predicting which patients will respond to which drugs
- 3) possibly distinguish between clinically significant and insignificant cancer to help limit the number of men being under- and over-treated
- 4) track cellular and molecular changes over time to quickly adapt treatment plans in response to changes
- 5) ensure the specific delivery of antibody drug conjugates (ADC) or radionuclide directly to the tumor(s) helping to limit the side-effects associated with current therapies
- 6) allow for the visualization of off-target delivery and exposure of therapeutics or radionuclides

Preclinical molecular imaging is key for effective translational research. And as such, there are various scaled down small animal single and multi-modality imaging tools to choose from.

PET/CT (computed tomography) and SPECT/CT are currently the most used imaging modalities for preclinical and clinical molecular imaging; however, other imaging tools like magnetic resonance imaging (MRI) and optical imaging (fluorescence and bioluminescence) are also available. Each imaging modality has unique advantages and disadvantages in terms of spatial resolution, sensitivity, cost and depth of tissue penetration [1, 17-21]. For example, the majority of PET isotopes are short lived (minutes to hours), with the exception of e.g. ⁸⁹Zr (half-life ~3 days) and thus requires a nearby cyclotron to generate positron-emitting isotopes. Quantification with SPECT can be cumbersome, although with recently developed software, like the computer-assisted diagnosis (CAD) software for automated bone scan index calculations, it is now possible to automatically detect and quantify the imaging data with 100% reproducibility in a very short time [22]. Both PET and SPECT, as single modalities, are limited by low spatial resolution. Anatomical localization can however be improved by coupling the two modalities to CT for coregistered imaging. MRI can produce excellent soft tissue images, but the sensitivity for ligand detection is low. Optical imaging on the other hand is inexpensive and easy to use, but it is limited by depth penetration. A comparison summary of currently used molecular imaging modalities is presented in Table 1 below.

IMAGING MODALITY	SOURCE OF IMAGE	TARGET	SENSITIVITY	SPATIAL RESOLUTION (MM)	DEPTH OF PENETRATION	QUANTITATIVE	CO-REGISTERED
Positron emission tomography (PET)	Annihilation photons (15 keV)-cylindrical detector rings	Physiological, molecular	pmol	Preclinical: 1-2 mm Clinical: 4-6 mm	Attenuation moderate	Yes	СТ
Single photon emission computed tomography (SPECT)	Gamma rays- collimation parallel or pin hole collimators	Physiological, molecular	nmol	Preclinical: 0.5-2 mm Clinical: 5-15 mm	Attenuation lower	Yes, more cumbersome	СТ
Magnetic resonance imaging (MRI)	Alterations in magnetic fields	Anatomical, Physiological	Low, can be improved by increasing magnetic field strength mmol	Preclinical: 10-100 μm Clinical: ~1 mm	Limitless	Yes	PET (new modality)
Optical fluorescence imaging	Visible or near infra-red light. Fluorophores, fluorochromes, or fluorescent dyes	Physiological, molecular	High, low signal to noise ratio	2-3 mm	<1 cm	Yes	Yes
Optical bioluminescence imaging	Visible or near infra-red light. Natural luminescent protein	Physiological, molecular	High, low signal to noise ratio	3-5 mm	1-2 cm	Yes	YES

Table 1. Molecular imaging modalities

Imaging with radiolabeled antibodies

The Society for Nuclear Medicine defines molecular imaging agents as "probes used to visualize, characterize and measure biological processes in living systems [17]". Molecular probes used in cancer imaging can range from antibodies and peptides to nanoparticles, quantum dots [19] and alpha particle emitting ion, like radium-223 [23]. All of these imaging probes could be discussed in great depth; however, in this dissertation the focus is on imaging prostate cancer with radiolabeled antibodies.

Radiolabeled monoclonal antibody (mAb)-based imaging provides the ideal platform for target imaging of prostate cancer due to their high specificity to detect virtually any tumor-associated and tissue-specific antigen [21]. In 1973, David Goldenberg first demonstrated that it was possible to target and image a human tumor antigen (CEA) in an animal model using a radiolabeled antibody [24, 25]. Five years later he went on to image a radiolabeled antibody in a human patient [25,127]. Since then, and with the advancements in preclinical and clinical imaging modalities, the development of hybridoma technology (which makes it possible to generate a unlimited number of antibodies against any kind of cellular target [25]) and the advancements in radiochemistry, imaging with radiolabeled antibodies has been revolutionized. Yet despite these advances, current imaging probes still lack the accuracy and specificity in detecting extraprostatic disease and today there is only one FDA approved radiolabeled mAb for imaging prostate cancer; Indium-111 (111In)-labeled Capromab pendetide (murine mAb 7E11-C5.3; ProstaScint®). The ProstaScint scan is a diagnostic imaging agent used to locate and determine the extent of prostate cancer in newly diagnosed patients. However, the accuracy is limited and scans are difficult to interpret since the antibody targets the intracellular epitope of prostate specific membrane antigen (PSMA), which is only exposed in dying or dead cells. The antibodies are also taken up in normal tissues like the gut, liver and kidneys [1, 26]. Nevertheless, PSMA is a valid tumor biomarker for prostate cancer, even though its true potential as a target antigen for prostate cancer imaging and therapy has not yet been made apparent in the clinical setting. There are now a number of new antibodies for PSMA directed against the extracellular domain under preclinical investigation or in clinical trials that show more promise; for example, 89Zr-Df-IAB2M for imaging metastatic prostate cancer [27] (www.clinicaltrials. gov; NCT01923727) and 89Zr-J591 in localized disease [28].

Monoclonal antibodies or immunoglobulin (Ig) are divided according to their molecular structure into five categories: IgG, IgA, IgM, IgD and IgE. The most typical Ig used for imaging cancer is the immunoglobulin G subclass, which can be further subdivided into four subclasses (or isotypes): IgG1, IgG2, IgG3 and IgG4. A schematic illustration of the basic structure of the IgG protein is shown in Figure 3.

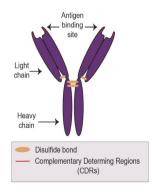


Figure 3. IgG1 mAb

The Ig is a Y-shaped protein consisting of two heavy chain (H) constant regions and two light chain (L) constant regions held together by disulphide bonds. The variable regions (antigen-binding sites) are located at the 'arms' or of the 'Y,' and each variable region contains three Complementarity Determining Regions (CDRs). The CDRs are the most variable parts of the antibody and it is their specific shape and size that determines which antigens the antibody will bind.

Prostate cancer is one of the most heterogeneous of all tumors and, it is quite possible that in order to target the whole tumor and metastases, one would require the use of multiple radiotracers. Multiple candidate targets for imaging cancer have now been characterized as a result of increased understanding of tumor biology. Yet finding the right target antigen and the right antibody for prostate cancer imaging remain a constant challenge. Antibodies suitable for target imaging of prostate cancer should have:

- 1) favorable antigen binding
- 2) good tumor penetration
- 3) a steady rate of clearance maintained from normal tissues
- 4) minimal immunogenicity for repeat administration [29-31]

Fortunately, mAbs can now be engineered from large display libraries as fully human or humanized antibodies designed to specifically recognize and attach to target proteins on the cell surface. However, the successfulness is not only dependent on the antibody used, but on the radiolabel chosen, and the target on the tumor and host [29]. A large number of radiolabeled antibodies have been successfully tested preclinically in small animal models; but only a limited number have reached the clinic. In this dissertation, I describe the use of four different radiolabeled antibodies to target prostate cancer. They are: (i) the human anti-Ku70/Ku80 antibody INCA-X, (ii) the murine anti-fPSA antibodies PSA-30 and (iii) 5A10 and (iv) the murine anti-ICAM-1 antibody R6.5.

Part III: Targets for Prostate Cancer Imaging

Sometimes the questions are complicated and the answers are simple. Dr. Suess

Prostate cancer biomarkers

Biomarkers are unique biological substances found in the blood, other fluids, or tissues that are used to indicate tumor(s) or abnormal processes in the body [32]. The ideal biomarker works by standing out in a cell. For example, by displaying a qualitative or quantitative alteration in gene or protein expression or by having an altered pathway from the normal cell of the same type. Prostate cancer biomarkers should be both sensitive and specific to the malignancy and found in tissues, the blood or urine in significantly abnormal concentrations that can be detected by an assay or imaging modality [33, 34]. Having the right biomarker can help to detect the cancer at an early stage, treat the patient with an individualized treatment plan and monitor the cancer at all stages. Moreover, a good biomarker can help to predict who needs treatment and is most likely to respond to that treatment, and if the treatment plan needs to be quickly adapted due to cellular changes [1, 34]. Currently, the best biomarker available for the early detection of prostate cancer is PSA, though a number of new biomarkers, like PSMA, prostate stem cell antigen (PSCA) and circulating tumor cells (CTCs) are emerging [34, 35]. In 2011, four reasons were defined as to why new biomarkers are needed in prostate cancer [36]. These are:

- 1) to improve cancer detection and staging
- 2) to identify subclasses of prostate cancer
- 3) to predict outcome after treatment
- 4) to select patients for different treatment options

In the first half of the 20th century, most men diagnosed with prostate cancer died since the cancer was detected from clinical symptoms at a late and often metastatic stage. In the 1990's, early diagnosis of prostate cancer in asymptomatic men was possible in part due to the increased use of assays that measure PSA in the blood [37, 38]. PSA is by far the most studied and used prostate cancer biomarker, yet it is far from a perfect biomarker. And as of May 2012, the U.S. Preventive Services Task Force (USPSTF) recommended against PSA-based screening in part due to the inability to distinguish between indolent and significant cancer [39]. Overall, the subject of serum based PSA testing remains a great source of debate among urologist and patient organizations and as such, there is a wide range of data both for and against its use in the clinic [40-45].

Tumors are very complex structures. Solid tumors are usually histologically heterogeneous making the search for the right antigen for target imaging difficult. Fortunately, because of our increased understanding of the basic biology involved in prostate cancer pathogenesis, many candidate biomarkers for prostate cancer imaging and therapy have now been identified. For this dissertation, three biomarker candidates – Ku70/Ku80, free PSA (fPSA) and ICAM-1 were investigated as possible targets for imaging prostate cancer with radiolabeled antibodies.

The target Ku70/Ku80

First characterized by Mimori et al. [46, 47] in 1981 as an autoantigen and possible serum marker for patients with polymyositis-scleroderma overlap syndrome, the Ku antigen was described as an acidic nuclear DNA-binding protein doublet involving at least two epitopes, Ku70 (XRCC6, 70 kDa) and Ku80 (XRCC5, 80 kDa). The Ku70/Ku80 protein complex is abundantly expressed in the nucleus of all cells where the main function is to recognize and repair DNA double strand breaks by non-homologous end-joining [48, 49]. Ku is thought to have a degree of plasticity in that it can bind to a range of double strand end breaks including: 3' or 5' overhangs, blunt ends and breaks produced by ionizing radiation [50]. Notably, the Ku proteins also play important roles in a plethora of other cellular processes including: V(D)J recombination [51], telomere maintenance [52-55], transcription regulation [56], possible receptor for DNA [57], carrier of proteolytic enzymes, integrin function [58] and apoptosis induction (cytosolic function) [59] (Figure 4).

The exact mechanisms behind all of the cellular roles is not yet fully understood; however, it is known to have both pro-survival and pro-invasive roles essential for tumor progression [58, 60, 61].

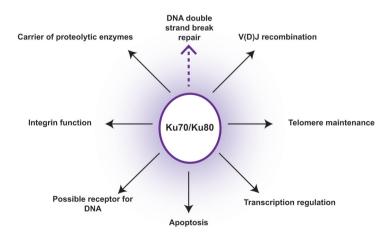


Figure 4: A Ku function chart. The dashed arrow indicated the major role.

Several studies have revealed that though Ku70/Ku80 is primarily a nuclear protein complex, it can also be found in the cytoplasm. And under certain conditions in various cell lines, including glioma cells, neuroblastoma cells and breast and prostate cancer cell lines, the antigen relocates to the plasma membrane [62, 63]. The change in location and expression seems to correlate with pathological state and tumor progression [64, 65]. On the cell surface, the complex is involved in cellular invasion, migration and cell adhesion [58, 61, 63, 66-68].

The essential and multifunction role of the Ku70/Ku80 complex and its relocation from the nucleus to the cell surface is what makes this antigen a candidate target for tumor imaging. Moreover, the relocation to the cell surface also creates a likely port for the delivery of ADCs or radionuclides directly to the tumor cells, potentially reducing the systemic toxicity associated with conventional treatments [61, 69].

The target free PSA

Prostate specific antigen (human kallikrein 3 [hK3, protein; or KLK3, gene]) is a human kallikrein-related peptidase highly specific to prostatic tissue [1, 70]. It is an androgen-regulated serine protease mainly produced by prostatic epithelium. Much lower levels of PSA expression have also been found in other normal and abnormal tissues; for example: pituitary gland, normal female breast and breast cancer, breast milk, lung cancer, salivary glands, apocrine sweat glands, thyroid and endometrium [71-76]. One biological role of PSA is to regulate semen coagulation by breaking up major gel forming proteins in seminal fluid.

PSA-based screening for early diagnosis of prostate cancer is widely used as a clinical marker and it does reduce mortality. However, because PSA is organ specific but not cancer specific it is limited by a substantial overlap in values between malignant and benign disease [1, 77]; and as such, is associated with a high risk of over detection of clinically insignificant prostate cancer [78].

Total PSA (tPSA) concentrations in the blood can rise for a variety of reasons including: age, BPH and prostitis. In the normal prostate, PSA is secreted in large amounts in the seminal fluid (0.3-3 mg/mL) as compared to the concentrations found in the blood, which is less than 4 ng/mL (as a reference level that is adjusted with age) [1, 79]. Elevated levels of PSA in the blood of a man with prostate cancer is not necessarily a result of the prostate cancer cells producing more PSA, but probably a consequence of changes in the prostate architecture; like a disrupted basal border and basement membrane resulting from disease progression [1, 3, 38, 80]. The architectural changes allow PSA to leak into the perivascular space and

circulation. Importantly for imaging, PSA is consistently produced and secreted at every stage of cancer including patients with castration resistant prostate cancer (CRPC) [80].

Early attempts to target PSA for imaging prostate cancer were trialed in both animal models and human studies [81-83]. However, those tests were conducted before it was discovered that PSA is found in two distinct forms in serum; namely, free (unbound) PSA (fPSA) and complexed (bound) PSA (cPSA) [84-87]. Complexed PSA forms bonds with protease inhibitors, which are largely produced in the liver and measured at high concentrations in blood. And as such, the early imaging results were hindered by high uptake in the liver and poor image quality due to high background activity. These failures were likely due to the fact that the antibodies used were polyclonal antibodies that were unable to distinguish between the different forms of PSA. Since those early tests, it is now known that targeting individual forms of the protein could yield much clearer and more tumor specific results.

PSA is initially produced as an inactive proenyzme ('pro' PSA) that is secreted from the intracellular space into the lumen where it is cleaved by another human kallikrein (human kallikrein 2) to yield catalytically active PSA. A portion of the active PSA can move into the blood stream where it rapidly and irreversibly forms a complex with a blood protease inhibitor (cPSA) [1, 80, 87, 88]. Alternatively, a portion of the active PSA can be converted to inactive PSA in the lumen by proteolysis, which can diffuse or leak into the blood serum as fPSA.

The majority of cPSA in blood serum is bound with alpha1-antichymotrypsin (60-90% [PSA-ACT]). The other complexes, alpha2-microglobulin (PSA-A2M) and alpha1-protease inhibitor (PSA-API), account for approximately 1-20 percent of the circulating protein [1, 70]. All four, fPSA, PSA-ACT, PSA-A2M and PSA-API are enzymatically inactive, yet all except PSA-A2M have immunoreativity and thus have antigens available for antibody binding [1, 89]. Free PSA in the serum can be found as 'pro' PSA, BPH-associated PSA (BPSA) and intact PSA (iPSA) [1, 90] (Figure 5).

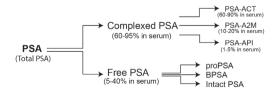


Figure 5. Molecular forms of prostate specific antigen (PSA). Adapted from McDougal 2012 [80].

Antibodies targeting tPSA for prostate cancer imaging has been shown to be suboptimal due to the antibodies binding to all molecular forms of the protein. However, we now have access to well-characterized isoform-specific antibodies that should, in theory, circumvent the problems of previous studies, like the high liver uptake and background noise. Therefore, we feel that by specifically targeting fPSA, which is located at high concentrations in close proximity to its site of production, we can increase the sensitivity and specificity of PSA as an imaging tool for prostate cancer. Additionally, fPSA is a promising candidate since concentrations found in the blood are much lower than cPSA and the epitope for fPSA is located within or adjacent to the catalytic cleft [88] making fPSA very specific for prostate cancer cells.

The target ICAM-1

Intercellular adhesion molecule-1 (ICAM-1) is a major adhesion molecule constitutively expressed in low concentrations in the membranes of leukocytes and endothelial cells and highly expressed on the cell surface of a variety of tumors, including human prostate cancer [91]. It is a member of the Ig supergene family composed of five homologous extracellular Ig-like domains [92]. ICAM-1 is a ligand for lymphoctye function-associated antigen 1 (LFA-1; a receptor found on leucocytes) [93] and is involved in cell-matrix and adhesion-dependent cell-cell interaction [94, 95]. Importantly, ICAM-1 is also involved in the pathogenesis of prostate cancer [95].

ICAM-1 expression is significantly increased in tumor cells and inflammatory cells when stimulated by inflammatory mediator cytokines like interleukin-1 (IL-1) and tumor necrosis factor alpha (TNF-alpha), thereby creating a tumor-related inflammatory microenviornment [9, 96, 97].

A study by Hayes and Seigel (2009)[91] compared the ICAM-1 expression on human tumors, metastases and normal tissue of 29 different tissues type. The investigators found ICAM-1 is not expressed in normal noncancerous areas of the prostate tissue but is expressed on the lymphoid cells infiltrating malignant and metastatic prostate tumors. Another study comparing gene expression variations in prostate cancer cell line [98] found ICAM-1 levels of expression are increased in androgen-insensitive cell lines, like the PC-3 and DU145 cell line more than they are in the androgen-sensitive cell lines like LNCaP cells. As noted earlier, studies are now suggesting that there is a link between prostate inflammation and prostate cancer and tumor progression [10, 99]. These findings indicate that ICAM-1 might be a marker for intra-tumoral inflammation that could be targeted to possibly distinguish between

the more and less aggressive prostate cancer [100]. It is also possible that ICAM-1 could be targeted to monitor patients as the tumors progress from hormone sensitive to CRPC (hormone insensitive) cancer. That, together with the fact that ICAM-1 is a cell surface protein involved in the pathogenesis of prostate cancer, is what make ICAM-1 an important candidate target for prostate cancer imaging with radiolabeled antibodies.

Part IV: The Present Investigation

A model is a lie that helps you see the truth. Howard Skipper

Aims

The main purpose of this work was to investigate three target antigens: Ku70/Ku80, fPSA and ICAM-1, as potential candidates for imaging and therapy of prostate cancer using radiolabeled antibodies. The studies were designed to assess the *in vivo* and *ex vivo* tumor targeting potential using prostate cancer based animal models. The studies were performed in prostate cancer cell lines and in tumor-bearing NMRI-nude and BALB/c-nude mice. Preclinical SPECT/CT and PET/CT *in vivo* imaging modalities, *ex vivo* multi-isotope digital autoradiography (DARG) and gamma-count measurements and immunohistochemistry (IHC) were used to achieve the aims of this dissertation.

Specific aims:

- Study the tumor targeting and biodistribution of ¹¹¹In-DTPA-INCA-X mAb to Ku70/Ku80 cell surface antigen in NMRI-nude mice bearing human prostate cancer xenografts. (I)
- Study of the tumor targeting and intra-tumoral antibody distribution of ¹²⁵I-PSA30 mAb to fPSA secreted antigen in NMRI-nude mice bearing human prostate cancer xenografts. (II)
- Investigate the impact mouse model immunogenic profiles have on the biodistribution of radiolabeled antibodies in NMRI-nude mice and BALB/c-nude mice bearing human prostate cancer xenografts. (III)
- Study the tumor targeting and intra-tumoral antibody distribution of ¹¹¹In-DTPA-R6.5 mAb and ¹⁷⁷Lu-DTPA-R6.5 mAb to ICAM-1 cell surface antigen in NMRI-nude mice bearing human prostate cancer xenografts. (IV)

General methods and materials

Ethical statement

All animal studies were approved and performed in strict accordance with the guidelines set by the Malmö-Lund Ethical Committee, Lund University for the use and care of laboratory animals. All efforts were made to strictly minimize animal suffering.

Human cell lines

The cell lines used in this dissertation are listed in Table 2 and explained in more detail below [101, 102].

Table 2.	Cell lin	ne description
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Cell lines	SITE OF ORGIN	DETAIL	TUMOROGENIC	ANDROGEN STATUS	ANDROGEN RECEPTOR (AR) STATUS	EXPRESSION RELEVANT TO STUDIES I-IV
Human PC-3 (Papers I and IV)	Bone metastasis; est. 1978	Genetically very stable classic cell line Mixed cell line of luminal, basal, intermediate, and neuroendocrine	Yes	Androgen independent	AR negative	+Ku70/Ku80 +ICAM-1
Human DU145 (Papers I-III)	Brain metastasis; est. 1977	Genetically very stable classic cell line Mixed cell line of luminal, basal, and intermediate	Yes	Androgen independent	AR negative	+Ku70/Ku80 -PSA
Human LNCaP (Papers II and III)	Lymph node metastasis; est. 1980	Genetically very stable classic cell line of luminal cell	Yes, but requires MatriGel (1:1)	Androgen dependent/ androgen stimulated	AR positive	+PSA
Human PC-3M (Paper I)	Derived from a liver metastasis removed from a mouse 6 weeks after injection of the parental PC-3 cell line into the spleen	Mixed cell line of luminal, basal, intermediate, and neuroendocrine	Yes	Androgen independent	AR negative	+Ku70/Ku80

All of the human cell lines used for this dissertation were purchased from ATCC (Manassas, VA, USA), with the exception of the human PC-3M-Lu2 cell line, which was purchased from Caliper (Hopkinton, MA). In Papers I and IV, the bone metastasis-derived PC-3 cells were chosen since they express the Ku70 and Ku80 antigens (I) and also ICAM-1 (IV). The PC-3M-Lu2 cell line is a metastatic clone of the PC-3 cells and was also used in Paper I since they express the Ku70 and Ku80 antigens. The brain metastasis-derived DU145 cells were used in Papers I and III. In paper I the cell line was chosen since it expresses the Ku70 and Ku80 antigens. In Papers III the DU145 cells were chosen as a control cell line since they do not express fPSA antigen. In Papers II and III the lymph node metastasis-derived LNCaP cell line was used since they express the fPSA antigen.

The PC-3 and DU145 cells were cultured as a monolayer in HAM's F12 (PC-3) or RPMI (DU145 and LNCaP) medium and supplemented with 10% FBS and 1% penicillin-streptomycin (PEST). PC-3M-Lu2 cells were cultured as monolayers in EMEM medium, supplemented with 10% heat inactivated FBS and 1% PEST. All cells were kept at 37°C in an atmosphere of 5% CO_2 . Cells were regularly tested for mycoplasma and tested mycoplasma free prior to animal inoculations.

Prostate tumor models

Male immunodeficient NMRI-nude mice (Taconic Europe [I, II and IV] or Charles River [III]) and BALB/c nude mice (Taconic Europe [III]) aged between 6-8 weeks old were used as a model. The tumor models were obtained by subcutaneous injection into the lower right flank (2-10 x 10⁶ cells per mouse) of PC-3 (I and IV), PC-3M-Lu2 (I), or DU145 (I and III) cells suspended in supplemented HAM's F12 medium or LNCaP (II and III) cell suspended in an equal mixture of RPMI 1640 supplemented medium and Matrigel.

The radiolabeled antibodies

INCA-X (I)

INCA-X (Bioinvent AB, Lund, Sweden) is a rapidly internalizing human IgG_1 mAb that recognizes cell surface exposed epitopes associated with the Ku70/Ku80 complex. INCA-X internalization after binding is via receptor-mediated endocytosis, which is a desirable trait for the delivery of toxins directly into the cancer cells. In 2006, Fransson and Borrebaeck [61] published a paper in which they showed INCA-X conjugated to Saporin had a very strong immunotoxic effect on human PC-3 cells (92% cell death).

PSA30 and 5A10 (II and III)

PSA30 and 5A10 are two murine IgG₁ mAbs that bind fPSA [103, 104]. The two antibodies have very similar binding characteristics and have been epitope mapped to a region in the 'kallikrein loop', which forms part of the protein active binding site [105]. Figure 6 is a 3-D model built from an investigation into the epitope binding of 53 PSA antibodies by the International Society of Oncodevelopmental Biology and Medicine (ISOBM) TD-3 PSA Workshop. It illustrates the locations of fPSA in the catalytic cleft and the binding sites for PSA30 (purple, ISOBM name code 73) and 5A10 (red, ISOBM name code 25)[105].

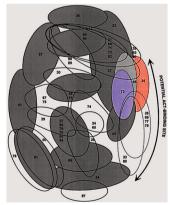


Figure 6. 3-D model of the epitope binding sites of 53 PSA antibodies by the International Society of Oncodevelopmental Biology and Medicine (ISOBM) TD-3 PSA Workshop [105].

When PSA forms a complex with ACT, PSA30 and 5A10 binding sites are masked, but the hidden epitopes are still available to target. Importantly, since PSA30 and 5A10 specifically bind an epitope in the catalytic cleft, molecules in the blood-pool are not targeted, thus resulting in better imaging quality since there would be less activity in circulation.

R6.5 (IV)

The mAb R6.5 (BIRR, Enlimomab; ATCC HB-9580TM) is a murine IgG_2 antibody specific to the extracellular domain 2 of the ICAM-1 molecule. R6.5 had previously been studied in a number of *in vitro* and *in vivo* models and has also been tested in clinical trials for refractory rheumatoid arthritis, stroke patients and organ transplant patients [106-110].

Antibody labeling

In order for the antibody-antigen binding to be visualized by an imaging modality, like PET or SPECT, the antibody must first be labeled with a radionuclide. The choice of label is an important aspect to consider since the radionuclide can affect the antibody biodistribution and binding properties. Radionuclides can be linked directly to the antibody, as in the case of iodine-125 (¹²⁵I)-labeled antibodies, or indirectly linked to the antibody, like in the case of ¹¹¹In- and Lutetium-177 (¹⁷⁷Lu)-labeled antibodies. Indirect labeling requires a chelate (or linker), for example DOTA or DTPA, to first be attached to the antibody before the radiolabel can be added. Metal ions like ¹¹¹In and ¹⁷⁷Lu are good radionuclides because they make residualizing labels, meaning they will be retained in the cell after the antibodies are catabolized. Whereas halogen chelates, like ¹²⁵I, are non-residualizing and are subsequently released from the cell after internalization. Radiochemistry techniques are continuously improving and fortunately there is now a large array of SPECT and PET radionuclides and chelators readily available. Below is a table describing the radionuclides used in this dissertation (Table 3).

Table 3. List of isotopes

Isotopes	Half-life	Decay mode (gamma energy, keV)	Imaging modality
Indium-111 (¹¹¹ In)	2.8 days	Electron capture (171 and 245)	SPECT
Lutetium-177 (¹⁷⁷ Lu)	6.7 days	β ⁻ (β energy 490 keV) (113 and 210)	SPECT
Iodine-125 (¹²⁵ I)	60 days	Electron capture (35,5)	SPECT
Fluorine-18 (¹⁸ F)	110 min	Positron (511)	PET

Imaging modalities

Multi-isotope Digital Autoradiography (II and IV): The intra-tumoral distribution of radioactivity was measured *ex vivo* using a double-side silicon strip detector with an intrinsic spatial resolution of 50 μ m (Biomolex 700 Imager, Biomolex, Oslo, Norway). Differences in both emission spectra and rate of decay were used to produce separate images of each radionuclide in animals administered more than one radionuclide.

SPECT/CT (II and III): All *in vivo* preclinical SPECT/CT imaging was accomplished using a dual modality NanoSPECT/CT plus preclinical scanner (Bioscan, Washington, DC). CT scans were acquired for anatomical co-registration for all animals before each whole-body SPECT images were obtained and without movement of the animal. Whole-body SPECT images were obtained using the NSP-106 multi-pinhole mouse collimator (each pinhole measuring 1 mm) and the data were reconstructed using HiSPECT software at standard setting (SciVis, Goettingen, Germany). In order to reduce noise, a Gaussian filter (FWHM 3 mm) was applied to all ¹⁷⁷Lu SPECT images.

PET/CT (IV): PET images were acquired using a dual modality PET/CT scanner (NanoPET/CT plus, Bioscan). CT scans were acquired for anatomical co-registration for all animals before each whole-body PET images and without movement of the animal.

*Both SPECT/CT and PET/CT images were analyzed using InVivoScope 2.0 software (inviCRO, Boston, MA, USA).

General results and discussion

The effect of tumor size and physical characteristics (I-IV)

Two general observations were noted with all four of the antibodies we tested. First, the tumor size does appear to affect the antibody uptake and intra-tumoral distribution. Second, the mAbs were mostly concentrated around the periphery of the tumor and perivascular regions and did not often penetrate deep into solid tumors. These observations however are not uncommon when working with full sized mAbs (150 kDa mass) [111, 112].

The first general observation regarding tumor size and the specific uptake of the radiolabeled antibody was simply that smaller tumors generally had a better specific uptake than the larger tumors. In larger tumors the antibodies tended to bind antigens around the viable tumor edges and vessels and/or pool in the necrotic area. Pooling in the necrotic areas of solid tumors is generally accepted to be a result of the enhanced permeability and retention effect (EPR) where the large antibodies are 'leaked' into the tumor and remain stuck in the necrotic areas [113].

The second general observation regarding limited tissue penetration into solid tumors could be down to a number of factors; however, the main culprits are most likely a binding site barrier and/or an internal physical barrier. A binding site barrier is seen either when high affinity antibodies bind strongly to the antigens at the tumor periphery and get stuck or when a low antibody dose is administered thus saturating the antigens and preventing deeper penetration [114]. Physical barriers are made by pathophysiological changes in the tumor. Tumor vessels, in general, are completely disorganized and abnormal both functionally and structurally. The vessels are often highly permeable ('leaky') and sometimes compress. These abnormal vessels, together with impaired lymphatic drainage, lead to uniformly elevated interstitial fluid pressure (IFP) inside the solid tumor [115]. In other words, there is extremely high pressure in the center of the tumor and low pressure towards the tumor periphery. The delivery of mAbs to the tumor is dependent more on transport by convection rather than diffusion and since the IFP is highly elevated in solid tumors, a barrier for fluid extravasation is created thus blocking the delivery of large molecules by opposing the inward flow [116-118]. This results in the only significant interstitial flow occurring at the tumor periphery where there is an outward oozing to the surrounding tissues [30]. But it is not only the abnormal vessels and elevated IFP that cause a problem. The antibody affinity, dose administered and speed of clearance could also affect the tumor penetration and should be points to consider

when choosing an antibody and organizing a study. For target imaging the antibody penetration into the tumor is not a huge problem; however, if we go further into targeted therapy, the depth of antibody penetration would need to be addressed.

In Papers II and IV, the multi-radionuclide DARG images and IHC illustrates the results of ¹²⁵I-PSA30 (II), ¹¹¹In-R6.5 (IV) and ¹⁷⁷Lu-R6.5 (IV) intra-tumoral distribution. In most cases, there was a clear EPR effect or binding site barrier preventing the antibody from penetrating deep into the tumor. However, it was not always the case. One animal bearing a PC-3 subcutaneous tumor (tumor size: 334 mm³) that was administered ¹¹¹In-R6.5 (IV) and sacrificed 72 hours post-injection, had very distinct specific uptake around the tumor periphery, but also very high activity in the viable cells located in the center, which correlated with high ICAM-1 expression (Figure 7).

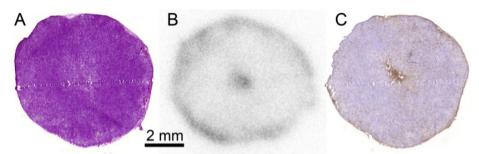


Figure 7. Adjacent tumor sections from an animal sacrificed 72 h post injection of the specific anti-ICAM-1 mAb 111In-R6.5. One stained with hematoxylin and eosin (A), one imaged using digital radiography to reveal the activity distribution (B) and one stained for immunohistochemistry detection of the ICAM-1 antigen (C). Activity image scaled from no (white) to max (black) measured activity per pixel.

In Papers I and III, the focus was on the antibody biodistribution in the whole animal and *in vivo* imaging; no DARG or IHC results are presented. First, we conducted pilot studies using ¹²⁵I-labeled INCA-X mAb and ¹²⁵I-labeled 5A10 mAb. Iodine-125 was chosen for the pilot studies since it is readily available, easy to use and can be directly attached to the antibody without the need of a chelator. Iodine-125 is a gamma-emitter that is an acceptable radionuclide for preclinical research, but it is not an optimal label for translation into a patient due to the long half-life (~60 days) and high absorbed dose. And unlike ¹¹¹In, which is trapped inside the target cell after internalization, ¹²⁵I breaks away from the antibody after internalization and is released back into circulation where it mainly accumulates as free ¹²⁵I in the thyroid.

In the original pilot studies, the intra-tumoral antibody distribution of both $^{125}\mbox{I-INCA-X}$ and $^{125}\mbox{I-5A10}$, as shown with DARG, correlated with what we present

in Papers II and IV. Namely, smaller tumors displayed better specific uptake of the radiolabeled antibodies, whereas in larger tumors the antibodies accumulated around the tumor peripheral and vessels and/or pooled in the necrotic areas. Figure 8 shows unpublished data from the ¹²⁵I-5A10 pilot studies, which gives a representative illustration of the antibody distribution in different size tumors.

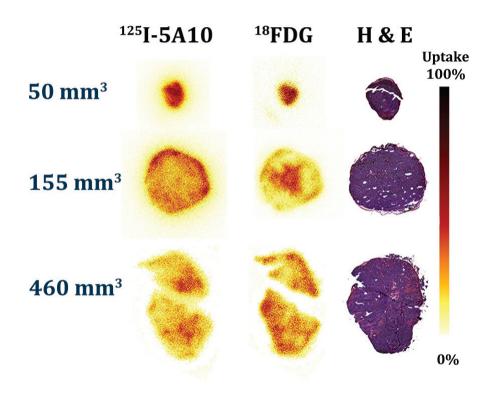


Figure 8. Multi-radionuclide digital autoradiography images from a silicon-strip detector based system separated by isotope. Individually normalized uptake of 125I-5A10 (48 h post-injection; 2.0-3.7 MBq/animal) and 18FDG (1 h post-injection) in LNCaP-based xenograph tumor sections. Nearby sections stained with H&E for histological analysis.

Radiolabeled antibodies versus clinical radiotracers

The metabolic tracer 2-[18F]fluoro-2-deoxy-D-glucose (18F-FDG) is one of the most widely used PET tracers in cancer imaging. It is a glucose analog that is taken up by cells in a similar fashion to unlabeled natural glucose, but it is not metabolized in the cell like natural glucose and is excreted by the kidneys into the urine [119]. Instead of being metabolized in the cell, ¹⁸F-FDG is phosphorylated to ¹⁸F-FDG-6-phosphate and effectively trapped. Studies have shown that in some cancers, the amount of ¹⁸F-FDG-6-phosphate trapped in the cell somewhat correlates with more aggressive tumors and larger areas of viable tumor cells [119, 120]. However, not all tumors are characteristically metabolic, which is particularly true for prostate cancer [120, 121]. For that reason, the metabolic probe [18F]fluorocholine (¹⁸F-choline, ¹⁸F-FCH) has had much more success in imaging prostate cancer. Choline is an element of the cell membrane phospholipids and a marker for imaging proliferation in cancer cells [121-123]. In cancer cells, the over-expressed choline kinase traps the labeled choline derivatives inside the cell thus providing information about the rate of lipid synthesis. It has also been reported that FCH mimics choline metabolism and sequestration by prostate cancer cells [122, 124]. In prostate cancer patients, ¹⁸F-FCH gives good imaging quality compared with ¹⁸F-FDG and provides improved detection of both locally advanced and metastatic disease [124]. Like ¹⁸F-FDG, ¹⁸F-FCH is also cleared via the kidneys and excreted in the urine.

In Papers II and IV, we conducted *ex vivo* multi-radionuclide DARG imaging of animals administered ¹²⁵I-PSA30 (II) or ¹⁷⁷Lu-R6.5 (IV) plus an ¹⁸F-labeled metabolic PET probe, FDG or FCH. In Paper II, DARG images showed the distribution of ¹²⁵I-PSA30 mAb in the LNCaP-based xenograft tumors did correlate with PSA expression, but did not correlate with areas of high ¹⁸F-FDG or ¹⁸F-FCH uptake in the same animal, except in areas of inflammation and necrosis. The metabolic probe, ¹⁸F-FDG, also accumulated in muscle, which was not the case for ¹²⁵I-PSA30. The antibody (PSA30) uptake in the necrotic areas was most likely a result of the EPR effect. The accumulation of the metabolic probe in areas of inflammations and in the muscle of animals allowed free movement post-injection is a well-known source of error to their use [119].

In Paper IV, DARG images of PC-3-based tumors showed ¹¹¹In-labeled and ¹⁷⁷Lulabeled R6.5 localized around vessels and in areas of less dense viable cells, which correlated with ICAM-1 antigen expression. The highest specific uptake was noted in areas with the strongest antigen stain that also contained clusters of vessels. Like the PSA30 mAb (II), radiolabeled R6.5 generally stayed around the tumor edges and did not penetrate deep into the tumor. That was not unexpected since the R6.5 mAb reportedly has a high avidity binding to cells, which could create a binding site barrier [125]. The ¹⁸F-FDG DARG images showed the highest specific uptake in tightly packed viable tumor cells. By contrast, the proliferation probe, ¹⁸F-FCH, somewhat correlated with radiolabeled R6.5 mAb specific uptake by accumulating in areas along the viable tumor periphery. Along with that, ¹⁸F-FCH also accumulated in necrotic areas (low activity) and towards the center of the tumors in regions containing densely packed tumor cells. Both ¹⁸F-FDG and ¹⁸F-FCH are small molecules that usually have no problem penetrating into solid tumors.

Along with the ARG results, in Paper IV, we also present *in vivo* multi-nuclide SPECT/CT and PET/CT results of animals co-injected with ¹⁷⁷Lu-R6.5 mAb and ¹⁸F-FDG or ¹⁸F-choline. Overall, the ¹⁸F-FDG PET/CT scans compared the best with the ¹⁷⁷Lu-R6.5 SPECT/CT scans of the same animal. This was unexpected since ¹⁸F-FCH usually performs better in human prostate cancer patients, but not unheard of in preclinical xenograft mouse models [126]. Interestingly, animals that received an additional injection of ¹⁸F-FCH had no clear specific uptake of activity in the tumor on the PET images, but activity accumulation in the liver, kidneys, bladder and general systemic circulation.

Imaging an internalizing antibody

In Paper I, we discuss targeting the Ku70/Ku80 antigen with the rapidly internalizing radiolabeled antibody, 111In-DTPA-INCA-X. This target and antibody have proved to be very interesting, yet also very complicated. The target itself is involved in many different cellular processes as shown in Figure 4 above and the antibody has been tested in various cancer cell lines. However, we were the first to investigate INCA-X mAb in an animal model. The major finding in Paper I was that in mice bearing human prostate cancer xenografts, the majority of activity was concentrated in the spleen of animals that only receive radiolabeled INCA-X. Yet, if the animals were first given an intravenously injected dose of unlabeled (cold) INCA-X, the off-target uptake was redirected to the tumor. This was a complete contradiction to our findings of the in vitro blocking tests conducted on the PC-3 cell line where the ¹¹¹In-DTPA-INCA-X mAb specific uptake was significantly blocked with a predose of cold INCA-X. This is a true example illustrating how the biological behavior of mAbs cannot always be predicted by *in vitro* studies. Nevertheless, INCA-X displays good localization properties in animals that first receive a predose of cold antibody and thus identify an antigen worth further investigation.

Immunological profile effect on the antibody biodistribution

As mentioned earlier, the choice of radiolabel can have a large affect on antibody binding properties. A recent study by Ulmert et al. (2012) [88] reported on the development of Zirconium-89 labeled 5A10 mAb (⁸⁹Zr-5A10). In that paper, they successfully showed that ⁸⁹Zr-5A10 specifically targets fPSA in prostate tumors and in bone metastases. The main downfalls of the ⁸⁹Zr-5A10 studies were the substantial liver uptake and transient tumor uptake, which could potentially under stage the tumor burden and complicate patient scheduling.

In order to fully explore 5A10 mAb as a potential antibody for targeting prostate cancer, we questioned whether or not changing experimental factors, like the radiolabel and mouse model, could improve the less favorable features of ⁸⁹Zr-5A10. We hypothesized that since mice do not naturally produce PSA, then the immunologic profile of the animal could affect the antibody kinetics and biodistribution. This is because animals with an intact (or partially intact) humoral immune system could produce competing PSA-antibodies, which could potentially block the exogenous tracer from targeting the antigen.

The ⁸⁹Zr-5A10 imaging studies were done using inbred BALB/c-nude mice so we also chose that model to test alongside the outbred NMRI-nude mice. The main difference in the animals is their immune profiles, i.e., BALB/c-nude mice have an intact humoral immune system, whereas the NMRI-nude mice do not. The isotope we chose to use was ¹¹¹In.

In comparison with the BALB/c-nude mice bearing LNCaP-based tumors, the biodistribution of ¹¹¹In-5A10 in the NMRI-nude with LNCaP-based tumors was much better. The liver uptake in NMRI-nude mice was significantly lower than that in the BALB/c nude mice (p=0.005) and in the NMRI-nude mice, the tumor accumulation increased over time (8.8 ± 2 %IA/g [injected dose per gram] at 24 h post-injection to 52±10.5 %IA/g at 72 h post-injection), whereas in the BALB/c mice, the tumor specific uptake remained fairly constant from 24 h to 72 h post-injection (24 h, 19.3±12.5 %IA/g; 72 h, 24.5±10.8 %IA/g) and then quickly dropped at 168 h post-injection.

In Paper III, we show that labeling strategies and the immunodeficiency status of the xenograft model can substantially impact the antibody biodistribution and should be parameters of consideration for the preclinical evaluation of experimental tracers for target imaging of cancer.

Final thoughts

In this dissertation we have described the tumor targeting and biodistribution properties of four different radiolabeled antibodies to three different prostate cancer associated antigens, as well as addressing some common problems associated with preclinical imaging. Preclinical imaging of prostate cancer is key for the transition from animal studies to man. However, as Howard Skipper said, "A model is a lie that helps you see the truth." There have been a large number of radiolabeled antibodies successfully demonstrated to selectively target cancer in preclinical animal models, yet only a few have reached the clinic. The results presented in Paper I and III show how important it is to know the limitations of your model. Specifically, in Paper I, we showed that *in vitro* data cannot always be translated into what you see in an animal model. Just as, preclinical imaging of radiolabeled antibodies administered to a mouse model cannot always reveal the true mechanism of action of that radiolabeled antibody in a man. In Paper III we went further to prove that the choice of radionuclide and immunological competence of the animal model could also affect the antibody biokinetics and biodistribution.

The heterogeneity of prostate tumors, along with a heterogeneous antigen production, can leave parts of a tumor without a target. So it could be that a collection of antibodies is needed as opposed to just one "magic bullet." There is an obvious need for new imaging probes and biomarkers for prostate cancer staging and for selecting and monitoring the most suitable therapies. Our *ex vivo* and *in vivo* investigations presented in this dissertation should act as support for further studies of the Ku70/Ku80, fPSA and ICAM-1 antigens. Future studies could include therapeutic applications and dosimetry studies to calculate the absorbed dose to the tumors and normal organs. The ultimate goal is to take an antibody from preclinical development to the clinical setting for both diagnostic and therapeutic purposes. Providing physicians with the best radiolabeled antibody (or selection of antibodies) gives them imaging tools that can better characterize and stage prostate cancer. Thus allowing the physician to individualize and adjust treatment plans for improved patient outcomes.

Acknowledgements

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Part VI: List of papers

It's very nice to be right sometimes. Nobel prize recipient Prof. Peter Higgs