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#### ORIGINAL RESEARCH

# A new approach to assess COPD by identifying lung function break-points

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**Purpose:** COPD is a progressive disease, which can take different routes, leading to great heterogeneity. The aim of the post-hoc analysis reported here was to perform continuous analyses of advanced lung function measurements, using linear and nonlinear regressions.

**Patients and methods:** Fifty-one COPD patients with mild to very severe disease (Global Initiative for Chronic Obstructive Lung Disease [GOLD] Stages I–IV) and 41 healthy smokers were investigated post-bronchodilation by flow-volume spirometry, body plethysmography, diffusion capacity testing, and impulse oscillometry. The relationship between COPD severity, based on forced expiratory volume in 1 second (FEV<sub>1</sub>), and different lung function parameters was analyzed by flexible nonparametric method, linear regression, and segmented linear regression with break-points.

**Results:** Most lung function parameters were nonlinear in relation to spirometric severity. Parameters related to volume (residual volume, functional residual capacity, total lung capacity, diffusion capacity [diffusion capacity of the lung for carbon monoxide], diffusion capacity of the lung for carbon monoxide/alveolar volume) and reactance (reactance area and reactance at 5Hz) were segmented with break-points at 60%–70% of FEV<sub>1</sub>. FEV<sub>1</sub>/forced vital capacity (FVC) and resonance frequency had break-points around 80% of FEV<sub>1</sub>, while many resistance parameters had break-points below 40%. The slopes in percent predicted differed; resistance at 5 Hz minus resistance at 20 Hz had a linear slope change of –5.3 per unit FEV<sub>1</sub>, while residual volume had no slope change above and –3.3 change per unit FEV<sub>1</sub> below its break-point of 61%.

**Conclusion:** Continuous analyses of different lung function parameters over the spirometric COPD severity range gave valuable information additional to categorical analyses. Parameters related to volume, diffusion capacity, and reactance showed break-points around 65% of FEV<sub>1</sub>, indicating that air trapping starts to dominate in moderate COPD (FEV<sub>1</sub>=50%–80%). This may have an impact on the patient's management plan and selection of patients and/or outcomes in clinical research.

**Keywords:** spirometry, severity, body plethysmography, single-breath carbon-monoxide diffusion test, impulse oscillometry, break-point

### Introduction

COPD is one of the leading causes of mortality around the globe and is the third cause of death.<sup>1</sup> It is characterized by irreversible progressive loss of lung function. The disease is heterogenic with two prominent characteristics, the first being airway inflammation and remodeling and the second being emphysema with airspace enlargement.<sup>2–5</sup> Diagnosis and Global Initiative for Chronic Obstructive Lung Disease (GOLD) grading of COPD is based on spirometry, while non-pharmacologic and pharmacologic management is based on symptoms, spirometry, previous exacerbations, and comorbidities.<sup>6,7</sup> Complementary methods are needed to further characterize

Correspondence: Göran Eriksson Respiratory Medicine and Allergology, Department of Clinical Sciences, Lund University, 221 84 Lund, Sweden Tel +46 733 299 929 Email goran.eriksson@med.lu.se the disease, both by volume and airflow restriction. Volume restrictions, due to emphysema formation and air trapping, are reflected by reduced forced vital capacity (FVC) but can be further characterized by using body plethysmography (bp).<sup>8</sup> We have previously shown that the combination of single-breath helium-diffusion carbon-monoxide diffusion testing together with body plethysmography can show valuable information about volume changes in COPD.<sup>9</sup> Flow restrictions can be read from the flow–volume spirometry curve shape,<sup>10</sup> but impulse oscillometry provides additional information.<sup>11–13</sup> Recruitment of small airways has been shown to be important for clinical outcomes like degree of dyspnea and possibly also risk of exacerbations.<sup>14</sup>

Classification of severity of airflow limitation is based on post-bronchodilator forced expiratory volume in 1 second (FEV<sub>1</sub>). Categorization into GOLD grades is valuable to communicate important information of different severity groups, and is a standard way of presenting data in numerous COPD publications.<sup>6,7</sup> However, continuous analysis can be a valuable complement, as it utilizes data more efficiently and can give additional information.

Our aim was to investigate if complementary advanced physiologic measurements analyzed in a continuous manner – linear, segmented linear with estimated breakpoints, and nonlinear regressions – could add to the understanding of the severity staging of COPD. The methodology of continuous analysis was applied on a dataset from our previous study.<sup>9</sup>

### Materials and methods

### Study participants

Smokers performed flow-volume spirometry and were classified as either healthy smoking controls (FEV,/FVC  $\geq$  0.7) or as COPD (FEV<sub>1</sub>/FVC <0.7) after bronchodilation. The COPD patients were further classified into GOLD Stages I, II, III, and IV. Study participants had no history of asthma, lung cancer, or any cardiorespiratory or respiratory disease. They had a smoking history of ≥15 pack years and no exacerbations or respiratory infections within the last 3 weeks. All participants performed the lung function tests at least 40 minutes after inhalation of a  $\beta_3$ -agonist and an antimuscarinic agonist. Participants inhaled salbutamol (400 µg Buventol® Easyhaler) and ipratropium (80 µg Atrovent® Handihaler) in the clinic except for seven patients who inhaled formoterol (9 µg within Symbicort® Turbuhaler) and tiotropium (18 µg Spiriva® Handihaler) at home in the morning. There were no restrictions on inhaled corticosteroids.

### Study design

This study was approved by the Regional Ethical Review Board in Lund (431/2008) and all study participants signed written informed consent. Study participants performed bp, with flow-volume spirometry (Jaeger® MasterScreen<sup>TM</sup> body plethysmograph; CareFusion [a subsidiary of Becton, Dickinson and Company, Franklin Lakes, NJ, USA]), impulse oscillometry system (Jaeger MasterScreen), <sup>15,16</sup> and single-breath helium-dilution carbon-monoxide diffusion test (CO; Jaeger MasterScreen Diffusion). All lung function measurements were done according to the manufacturer's instructions and according to European Respiratory Society/American Thorax Society recommendations. <sup>8,10,17</sup> Established reference values by Crapo et al were used. <sup>18</sup>

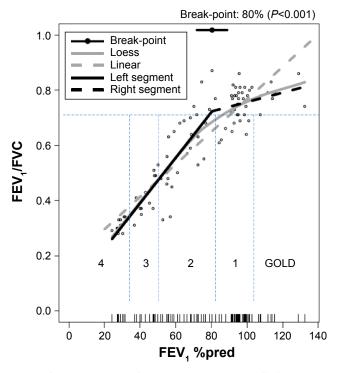
### **Statistics**

For descriptive purposes, medians and interquartile ranges were used. The detection of potential break-points was performed by a regression model allowing for segmented relationships. 19,20 In a given linear regression (LR) model, the method tries to estimate a new model having a segmented (or broken-line) relationship. This is defined by the slope of the parameter(s) and the break-point(s) where the linear relation changes. The method gives point estimates and approximate standard errors of the model parameters, including the break-points. In Figure 1, an example is given on the relationship between FEV, percent of predicted (%pred) and FEV<sub>1</sub>/FVC. The estimated break-point is shown as a circle at 80% of FEV, with the associated 95% confidence interval (horizontal line through the circle in the top of the figure). The solid black line to the left and the black hatched line to the right of the break-point are the corresponding segmented linear regression (SLR) technique fits with different slopes and joined at the break-point. An ordinary LR line (gray hatched) and the reference, a nonparametric fit by the local regression (LOESS) line (gray solid) are also displayed.<sup>21</sup> The method allows for several break-points, but the investigation presented here only focused on trying to find one break-point. All calculations, where not otherwise specified, were performed in (v 3.1.1) and SPSS (v 22) software.

### Results

### Subject characteristics

In total, 92 subjects were included in the study, of whom 41 were classified as healthy smokers (FEV<sub>1</sub>/FVC  $\geq$ 0.7) and 51 as COPD patients. The COPD group was then classified according to GOLD Stages I–IV: Stage I, n=9; Stage II, n=21; Stage III, n=14; and Stage IV, n=7.6,7 The demographic data



**Figure 1** A descriptive example of the segmented linear regression (SLR) relationship between forced expiratory volume in 1 second (FEV<sub>1</sub>) percent of predicted (%pred) and FEV<sub>1</sub>/forced vital capacity (FVC), showing an estimated break-point at 80% of FEV<sub>1</sub> when the FEV<sub>1</sub>/FVC ratio is close to 0.70.

**Notes:** The solid line to the left (SLR-L) and the hatched line to the right (SLR-R) of the break-point are the segmented linear fits which join at the break-point, estimated at the top of the figure (circles with the associated 95% confidence intervals). An ordinary linear regression (LR) line (hatched gray) and the reference, a nonparametric fit by the local regression (LOESS) method (gray line), are also displayed. Dots show the values of each healthy smoker and COPD patient. The Global Initiative for Chronic Obstructive Lung Disease (GOLD) stages and the obstructive FEV,/FVC ratio of 0.70 are also shown.

between groups were well matched, while disease-related baseline data (smoking, symptoms, FEV<sub>1</sub>%pred, and prescribed medication) varied according to severity (Table 1).

### Curve fittings of different lung function parameters related to FEV<sub>1</sub>%pred

The different lung function parameters showed different curve shapes as a function of  $\text{FEV}_1$ %pred. The examples in Figure 2 were selected and arranged by P-value for the segmented test (from no P-value to P<0.001) showing that as the P-value became lower, the SLR curve fitting appeared more closely aligned to LOESS, as our reference, than the LR curve fitting. This appeared applicable even if the P-value was in the range of 0.05 to 0.30.

Data for all lung function parameters and their fit to LR and SLR can be seen in Table 2.

The following lung function parameters in absolute values or %pred were best described by SLR; that is, the segmented test showed P-values <0.05: FEV $_1$ /FVC, FEV $_1$ /FVC%pred, total lung capacity (TLC) %pred, functional residual capacity (FRC), FRC%pred, RV $_{bp}$ (RV that is measured by bodyplethysmography), RV $_{bp}$ %pred, RV $_{bp-CO}$ %pred, total resistance ( $R_{tot}$ ),  $R_{tot}$ %pred, inspiratory resistance ( $R_{in}$ ), expiratory resistance ( $R_{ex}$ ), diffusion capacity of the lung for carbon monoxide (DLCO), DLCO%pred, DLCO/alveolar volume (VA), DLCO/VA%pred, resistance at 5 Hz (R5), R5 minus R20, reactance area (AX), resonance frequency ( $F_{res}$ ), and reactance at 5 Hz (X5).

Table I Patient characteristics

Characteristic	Healthy smokers (n=41)	GOLD stage				
		I (n=9)	II (n=21)	III (n=14)	IV (n=7)	
Age, years (range)	ge, years (range) 68 (66–70)		65 (61–69)	66 (62–70)	66 (62–74)	
Smoking, pack years (range)	27 (21–36)	32 (19–50)	31 (23-52)	46 (30–53)	30 (20-40)	
Females/males	17/24	6/3	12/9	4/10	5/2	
Smoker/former smoker, n	5/36	7/2	7/14	1/13	0/7	
FEV, L (range)	3.0 (2.4-3.4)	2.5 (2.1-3.1)	1.8 (1.3-2.2)	1.3 (1.0-1.6)	0.7 (0.6-0.9)	
FEV %pred (range)	95 (92–102)	92 (86–99)	59 (55–69)	41 (35–47)	28 (27–29)	
FVC, L (range)	3.9 (3.1-4.4)	3.8 (3.1-4.6)	3.2 (2.8-3.9)	3.3 (3.0-3.8)	2.2 (1.9-3.0)	
FVC%pred (range)	96 (89–101)	109 (107–113)	89 (75–98)	77 (73–87)	70 (65–77)	
FEV <sub>1</sub> /FVC (range)	0.77 (0.74-0.81)	0.66 (0.63-0.69)	0.55 (0.48-0.64)	0.37 (0.34-0.45)	0.30 (0.29-0.33)	
BMI, kg/m <sup>2</sup> (range)	27 (24–29)	26 (25–28)	25 (22–30)	24 (22–27)	24 (23–30)	
No inhaled medication, n	39	8	4	1	0	
ICS, n	2	1	13	11	6	
SABA, n	_	_	8	7	2	
LAMA, n	1	1	13	13	7	
LABA, n	2	1	12	10	6	
CCQ score (range)	4 (2–7)	8 (3-13)	12 (5–18)	19 (14–28)	17 (9–17)*	

Notes: \*CCQ score from only two of the GOLD Stage IV patients. Data are presented as median (interquartile range).

**Abbreviations:** %pred, percent of predicted; BMI, body mass index; CCQ, Clinical COPD Questionnaire; FEV, forced expiratory volume in 1 second; FVC, forced vital capacity; GOLD, Global Initiative for Chronic Obstructive Lung Disease; ICS, inhaled corticosteroids; IQR, InterQuartile range; LABA, long-acting  $\beta_2$  agonist; LAMA, long-acting muscarinic agonist; SABA, short-acting  $\beta_2$  agonist.

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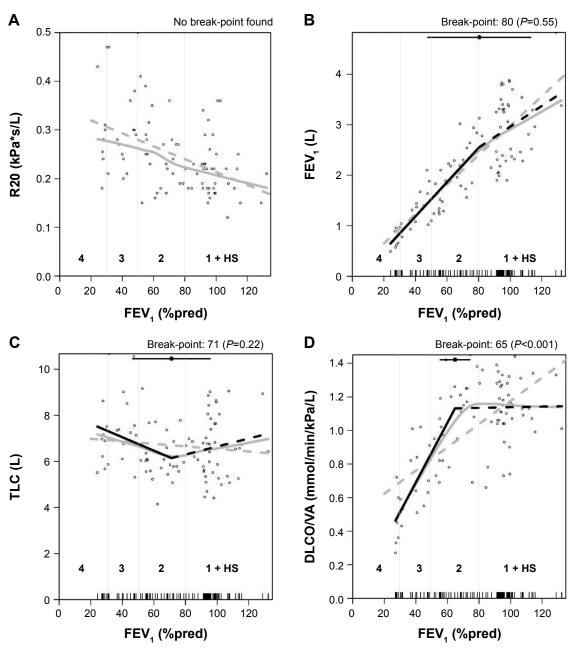


Figure 2 The relationship between spirometric severity (forced expiratory volume in 1 second [FEV,1] percent of predicted [%pred]) and selected lung function parameters: (A) resistance at 20 Hz (R20), (B) FEV,, (C) total lung capacity (TLC), and (D) diffusion capacity of the lung for carbon monoxide (DLCO)/alveolar volume (VA).

Notes: Figures are arranged by P-values for the segmented test (from no P-value in A to P<0.001 in D). The lower the P-value, the better the segmented linear regression (SLR) curve fitting aligned to local regression (LOESS) compared to the linear regression (LR) curve fitting. The black solid line to the left (SLR-L) and the black hatched line to the right (SLR-R) of the break-point are the segmented linear fits which join at the break-point, estimated at the top of the figure (circles with the associated 95% confidence intervals). An ordinary LR line (hatched gray) and the reference, a nonparametric fit by the LOESS method (solid gray), are also displayed. Dots show the values of each healthy smoker and COPD patient. Bolded letters between lines indicate Global Initiative for Chronic Obstructive Lung Disease (GOLD) stage and healthy smokers (HS).

The following lung function parameters were best described by LR (defined as segmented test P>0.05): FEV<sub>1</sub>, FEV<sub>1</sub>%pred, FVC, FVC%pred, inspiratory capacity (IC), IC%pred, TLC, RV<sub>CO</sub> (RV measured by CO-diffusion), RV<sub>co</sub>%pred, VA, VA%pred, R5%pred, R20, R20%pred, R5-R20%pred, and X5%pred.

In most cases, the segmented test defined the same curve fitting (SLR or LR) for parameters where both absolute value

and %pred were determined, indicating that sex, age, and body size did not strongly influence the results. TLC, R5, R5-R20, and X5 were exceptions. TLC had a similar break-point as TLC%pred (71% and 69% predicted, respectively) and followed LOESS well, even though the segmented test defined TLC as having a preferred linear slope (Figure 2C and Table 2).  $R_{tot}$  and  $R_{tot}$ %pred showed the biggest discrepancy between the two significant break-points (61 and 31, respectively).

Table 2 Linear regression (LR) and segmented linear regression (SLR) slopes

Method	Parameters	LR or SLR	Segmented test, P-value	LR slope	SLR-L slope	Break-point (FEV <sub> </sub> %pred)	SLR-R slope
bp	FEV	LR	0.600	0.029***	0.030***,#	95.0	0.010 ns#
	FEV %pred	LR	1.000	1.000***	nd	nd	nd
	FVC	LR	0.500	0.016***	0.123 ns#	33.0	0.012**,#
	FVC%pred	LR	0.100	0.400***	0.300***	96.0	0.800***
	FEV <sub>I</sub> /FVC	SLR	<0.001	0.006***	0.008***	80.0	0.002***
	FEV <sub>1</sub> /FVC%	SLR	< 0.001	0.600***	0.800***	80.0	0.200 ns
	TLC	LR	0.200	-0.060 ns	-0.029 ns	71.0	0.017 ns
	TLC%pred	SLR	<0.001	-0.200*	-0.800***	69.0	0.400*
	RV	SLR	<0.001	-0.023***	-0.07I***	62.0	0.003 ns
	RV%pred	SLR	<0.001	-1.100***	-3.300***	62.0	0.050 ns
	FRC	SLR	<0.001	-0.025***	-0.066***	65.0	0.002 ns
	FRC%pred	SLR	<0.001	-0.800***	-2.300***	65.0	0.100 ns
	IC .	LR	1.000	0.013**	nd	nd	nd
	IC%pred	LR	0.060	0.600***	2.100 ns#	39.0	0.400***,#
	R <sub>tot</sub>	SLR	<0.001	-0.078***	-0.175***	61.0	-0.030 ns
	R <sub>tot</sub> %pred	SLR	<0.001	-2.500***	-38.600***	31.0	-1.800***
	R <sub>ex</sub>	SLR	< 0.050	-0.177***	-3.234*	32.0	-0.124***
	R <sub>in</sub>	SLR	<0.001	-0.035***	-0.079***	32.0	-0.025***
со	DLCO	SLR	< 0.050	0.049***	0.089***	68.0	0.019 ns
	DLCO%pred	SLR	0.010	0.600***	1.100***	64.0	0.300***
	DLCO/VA	SLR	<0.001	0.007***	0.018***	65.0	0.000 ns
	DLCO/VA%pred	SLR	<0.001	0.500***	1.200***	70.0	−0.060 ns
	$RV_CO$	LR	1.000	0.004***	nd	nd	nd
	RV <sub>co</sub> %pred	LR	1.000	0.200*	nd	nd	nd
	VA	LR	0.660	0.017***	0.171 ns#	32.2	0.013****#
	VA%pred	LR	0.600	0.300***	0.200*,#	79.0	0.400**,#
bp-CO	$RV_{bp}$ - $RV_{CO}$ %pred	SLR	<0.001	-I.300***	-3.600***	62.0	-0.100 ns
IOS	AX	SLR	< 0.010	-0.029***	-0.059***	65.0	-0.010 ns
	F <sub>res</sub>	SLR	< 0.050	-0.170***	-0.24I***	79.0	−0.057 ns
	R20	LR	1.000	-0.001***	nd	nd	nd
	R20%pred	LR	0.800	-0.400***	0.030 ns#	47.0	-0.500**** <sup>#</sup>
	R5	SLR	< 0.001	-0.004***	-0.184***	27.0	-0.003***
	R5%pred	LR	1.000	-1.100***	nd	nd	nd
	R5-R20	SLR	< 0.001	-0.003***	-0.141***	27.0	-0.002
	R5-R20%pred	LR	1.000	-5.300***	nd	nd	nd
	X5	SLR	<0.001	0.003***	0.009***	61.0	0.001 ns
	X5%pred	LR	0.300	-8.100***	-I2.700***,#	74.0	-2.500 ns#

Notes: The LR and SLR regression slopes are presented for all lung function parameters in absolute values and % predicted. The preferred regression method (LR or SLR), with its data, is presented in bold text and is based on the segmented test P-value (LR in case of P>0.05 and SLR in case of P<0.05). LR has one slope, while SLR has a slope to the left (SLR-L) and to the right (SLR-R) of a break-point (in FEV<sub>1</sub>%pred). \*P<0.05, \*\*P<0.01, \*\*\*P<0.001, and ns = P>0.05 depict the significance of the slopes compared to a horizontal line. nd = the SLR method failed to identify a break-point. "No significant difference (P>0.05) between SLR-L and SLR-R, further supporting the selection of LR. **Abbreviations**: %pred, percent of predicted; AX, reactance area; BMI, body mass index; bp, body plethysmography; CO, single-breath helium-dilution carbon-monoxide diffusion test; DLCO, diffusion capacity of the lung for carbon monoxide; FEV<sub>1</sub>, forced expiratory volume in I second; FRC, functional residual capacity;  $F_{res}$ , resonance frequency; FVC, forced vital capacity; IC, inspiratory capacity; ICS, inhaled corticosteroids; IOS, impulse oscillometry system; nd, not detected; R5, resistance at 20 Hz;  $F_{res}$ , expiratory resistance;  $F_{res}$ , total resistance; RV, residual volume; RV<sub>bp</sub>, RV measured by bp; RV<sub>CO</sub>, RV measured by CO; TLC, total lung capacity; VA, alveolar volume; X5, reactance at 5 Hz; ns, not significant.

### Break-points for parameters with segmented curve fittings

Break-points in the range of 60–70 FEV $_1$ %pred were seen for several of the lung function parameters (Table 2): TLC%pred, FRC, FRC%pred, RV $_{bp}$ , RV $_{bp}$ %pred, RV $_{bp-CO}$ %pred, R $_{tot}$ , DLCO, DLCO%pred, DLCO/VA, DLCO/VA%pred, AX, and X5.

There was good agreement for the break-points between absolute and predicted values, where both were determined, indicating that sex, age, and body size do not strongly influence the results. The parameters with a break-point in the range of 60–70% FEV<sub>1</sub>%pred were all related to volume, diffusion capacity or reactance. In Figure 3, four volume-related parameters, one diffusion capacity

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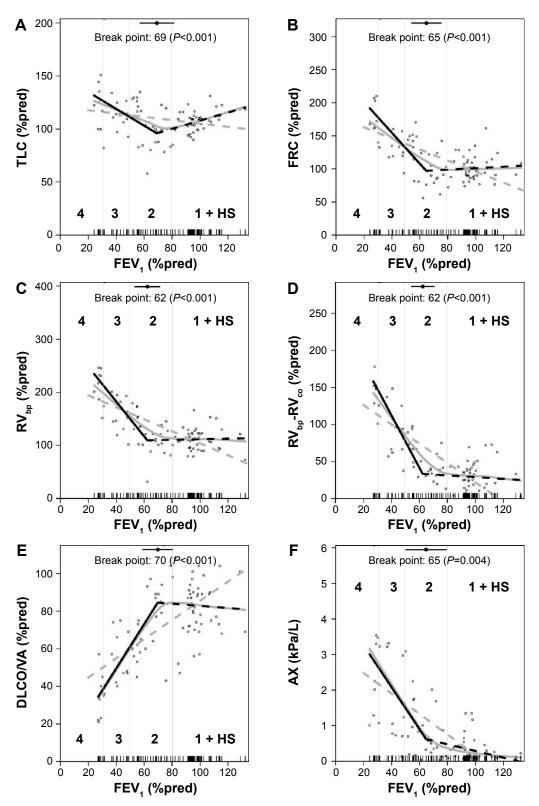


Figure 3 The relationship between spirometric severity (forced expiratory volume in I second [FEV] percent of predicted [%pred]) and selected lung function parameters with break-points in the range of 60–70 FEV<sub>1</sub>%pred. Total lung capacity (TLC) %pred (**A**), functional residual capacity (FRC) %pred (**B**), RV<sub>bp</sub>%pred (**C**), RV<sub>bp</sub>RV<sub>CO</sub> %pred (**D**), diffusion capacity of the lung for carbon monoxide (DLCO)/alveolar volume (VA) %pred (**E**), and reactance area (AX) (**F**) all had break-points in the middle of Global Initiative for Chronic Obstructive Lung Disease (GOLD) Stage II.

Notes: The black solid line to the left (SLR-L) and the black hatched line to the right (SLR-R) of the break-point are the segmented linear fits which join at the break-point, estimated in the top of the figure (circles with the associated 95% confidence intervals). An ordinary linear regression (LR) line (hatched gray) and the reference, a nonparametric fit by the local regression (LOESS) method (solid gray), are also displayed. Dots show the values of each healthy smoker and COPD patient. Bolded letters between lines indicate GOLD stages and healthy smokers (HS).

**Abbreviations:** RV<sub>bo</sub>, Residual Volume measured with bodypletysmograph; RV<sub>CO</sub>, RV measured by CO.

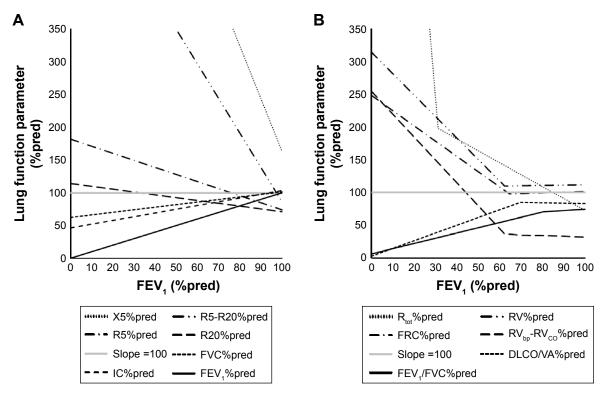


Figure 4 Descriptive presentation of lung function parameters expressed as percent of predicted (%pred) in relation to forced expiratory volume in 1 second (FEV<sub>1</sub>) %pred for healthy smokers and COPD patients. (A) Preferred linear regression (LR) lines and (B) segmented linear regression (SLR) lines.

Note: The gray line shows an estimation of a slope of 1 at 100% predicted.

**Abbreviations:** DLCO, diffusion capacity of the lung for carbon monoxide; FRC, functional residual capacity; FVC, forced vital capacity; IC, inspiratory capacity; R5, resistance at 5 Hz; R20, resistance at 20 Hz; R<sub>tot</sub>, total resistance; RV<sub>bp</sub>, Residual Volume measured with bodypletysmograph; RV<sub>CO</sub>, RV measured by CO; VA, alveolar volume; X5, reactance at 5 Hz

parameter, and one impulse oscillometry system parameter are displayed.

Break-points around 80 FEV  $_{\rm l}$  %pred were seen for three lung function parameters (Table 2): FEV  $_{\rm l}/{\rm FVC}$  %pred, and F  $_{\rm rec}$ .

Break-points below 40 FEV $_1$ % were seen for five lung function parameters (Table 2):  $R_{_{10}}$ % pred,  $R_{_{1n}}$ ,  $R_{_{ex}}$ , R5, and R5-R20.

There was no good agreement between SLR curves with break-points below 40 FEV<sub>1</sub>% and the LOESS fitting, as these steep slopes below the break-points were not picked up by the LOESS.

## Descriptive presentation of slopes for parameters expressed as percent of predicted

FEV<sub>1</sub>%pred versus FEV<sub>1</sub>%pred showed a positive linear slope of 1.0 and other lung function parameters (in %pred values) can be related to FEV<sub>1</sub>%pred and to each other (Figure 4). IC%pred and FVC%pred also had positive linear slopes of 0.6 (P<0.001) and 0.4 (P<0.001) respectively. R5-R20%pred, X5%pred, R5%pred, and R20%pred showed negative linear slopes: -5.3 (P<0.001), -8.1 (P<0.001), -1.1 (P<0.001), and -0.4 (P<0.001), respectively (Figure 4A).

Figure 4B shows segmented parameters. FEV<sub>1</sub>/FVC%pred and DLCO/VA%pred had significant positive slopes (0.8 and 1.2, respectively, both P < 0.001) below their respective break-point. FEV<sub>1</sub>/FVC%pred and DLCO/VA%pred showed nonsignificant horizontal slopes above their break-points. FRC%pred, RV<sub>bp</sub>%pred, and RV<sub>bp-CO</sub>%pred all had negative slopes below their break-points: -2.3 (P < 0.001), -3.3 (P < 0.001) and -3.6 (P < 0.001), respectively. Above their break-points they all showed nonsignificant slopes. R<sub>tot</sub>%pred had a significant positive slope (-38.6, P < 0.001) below its break-point as well as above (-1.8, P < 0.001). TLC%pred showed a different pattern by having a significant negative slope of -0.8 (P < 0.001) below its break-point and a significant positive slope of 0.4 (P < 0.05) above.

### **Discussion**

In this post-hoc analysis we analyzed lung function data in relation to spirometric COPD severity, using the classification of severity of airflow limitation. <sup>6,7</sup> However, the data were analyzed as continuous data, instead of categorically. Three different regression models were used: a linear, a segmented linear, and a flexible nonparametric fit method. The applied continuous analyses gave information for each lung function

parameter about (1) the curve shapes in the whole population from healthy smokers to subjects with very severe COPD, (2) estimated break-points, (3) the slope changes above and below estimated break-points, and (4) the slope expressed as change per unit FEV<sub>1</sub>%pred for comparison between different parameters. This approach can bring new and valuable information to the understanding of COPD heterogeneity.

Some lung function parameters, for example, FVC%pred and IC%pred, had a linear significant slope through the whole FEV<sub>1</sub>%pred spectrum. However, several parameters were nonlinear in relation to FEV<sub>1</sub>%pred, which were supported by both the descriptive LOESS and the statistically significant segmented regression fits with significant break-points.

The FEV<sub>1</sub>/FVC value was 0.7 at the break-point of 80% of FEV, %pred, which was logical, as two different populations were recruited into the study. The ratio for healthy smokers (>0.7) showed a nonsignificant slope change of 0.2 per unit  $FEV_1$ %pred, while the ratio for the COPD group (<0.7) had an increased slope change of 0.8 per unit FEV, %pred. This increase in obstruction, below the well-accepted cutoff point of 0.7, was similar to the increase in spirometric severity. An interesting finding was that several different parameters from different methods had break-points between 60% and 70% of FEV, %pred; that is, in the middle of GOLD Stage II. For example the three volume-related parameters from bp (RV<sub>bm</sub>%pred, FRC%pred, and TLC%pred) showed only small volume changes above their break-points, while the volume increased significantly below their break-points. The volume-related parameters (RV<sub>bn</sub>%pred, RV<sub>bn-CO</sub>%pred, and FRC%pred) increased two- to fourfold per unit fall in FEV<sub>1</sub>%pred. These parameters are strongly related to air trapping and our data suggest that a change in the lung parenchyma occurs in the middle of GOLD Stage II. Similarly, the diffusion capacity showed break-point values from 60%-70% of FEV, %pred, irrespective of whether DLCO was calculated as absolute or %pred or with or without correction for VA. Our findings thereby demonstrate that reduced gas diffusion capacity and increased air trapping occurred in parallel. Finally the two reactance parameters, AX and X5, also had break-points between 60% and 70% of FEV<sub>1</sub>. Reactance is suggested to reflect elasticity of the parenchyma and is associated with air trapping and differs from resistance, which is measuring airway obstruction.<sup>13</sup> Individual patients may have early or late onset of lost diffusion capacity and/or increased air trapping and extended lung function tests may be specifically valid in GOLD Stage II patients.

Resistance showed either a linear curve fitting over the whole spectrum of FEV %pred (R5%pred, R20 and R20%pred, R5-R20%pred) or a segmented curve fitting with a break-point of less than 40% of FEV<sub>1</sub>%pred (R<sub>tot</sub>%pred, R<sub>in</sub>, R<sub>ex</sub>, R5%pred, R5-R20). The low break-points of 25%–40% are interesting but should be regarded with caution. They could have a physiologic/pathologic explanation – for instance, destruction and collapse of the airways in this very severe group of COPD. A more plausible explanation could be that the data were driven by few individuals and/or the methods reached their lower limit for accurate measures.

The contribution of the regional resistances to the total resistance in the range from healthy smokers down to subjects with severe COPD is interesting. The total resistance, represented by R5%pred and R<sub>tot</sub>%pred (above break-point), had a slope change of –1.1 and –1.8 per unit of FEV<sub>1</sub>%pred, respectively. The regional slope change was small for the central resistance (R20%pred =–0.4 per unit FEV<sub>1</sub>%pred), while the peripheral slope change (R5-R20%pred) decreased fivefold per unit FEV<sub>1</sub>%pred in the whole range of COPD. The high increase of the peripheral resistance at lower lung function has been discussed,<sup>22</sup> but Hogg et al summarize elegantly this phenomenon as a combination of the narrowing/collapse and destruction of the small airways.<sup>23</sup>

Our data support the sequence of tissue destruction in COPD. Firstly, toxic particles destroy the terminal bronchioles, indicated early on by the change in peripheral resistance. <sup>12,13</sup> Secondly, limitation in gas exchange and increase of hyperinflation follow predominantly in the middle of GOLD Stage II. Emphysema also comes gradually but the collapse of entire lung lobules and coalescence of many lobules occur later, <sup>23</sup> maybe below 40%, as our data may indicate.

Our findings may have clinical implications related to the management of patients. Today's guidelines advocate spirometry to diagnose (FEV<sub>1</sub>/FVC) and define severity (FEV<sub>1</sub>%pred) in every patient. A severity grading by only spirometry may miss the small-airway destruction phenotype, the severe gas-exchange mismatch phenotype, and the severe air trapping phenotype. Today's guidelines have moved away from FEV, as the only determinant for choice of therapy and recommend a more holistic treatment strategy including symptoms, lung function, and previous exacerbations.<sup>6,7</sup> However, the cutoff point of an FEV<sub>1</sub> of 50%pred does not address the heterogeneity in GOLD Stage II (50%-80% predicted). We think that a better classification of mild to moderate COPD could differentiate the phenotypes, which need different management plans, and stimulate more personalized management.

Our findings also indicate that clinical and pharmaceutical research should extend the characterization of COPD patients and specifically GOLD Stage II patients. A suggestion would be to expand baseline characterization to report small-airway disease (for example R5-R20), air-trapping (for example RV) and gas exchange (for example DLCO) for each GOLD stage. The advantage would be that subgroup responses to different investigations (tests or interventions) might lead to better understanding of COPD and better management and use of present as well as future treatments.

### Limitations and future directions

This study has generated new valuable information. However, to validate our data, more subjects, especially healthy nonsmokers and mild and very severe COPD patients should be included. The healthy nonsmokers may have changed the slopes marginally but most likely positively for the interpretation. The low number of very severe COPD patients makes our interpretation in this range speculative, as this could be a methodological problem. An interesting angle would have been to see where in this regression model the new classification, including exacerbation frequency and dyspnea, would fit in and if it would help, to some extent, to divide GOLD Stage II the same way as the break-points do. A two-segmented regression model could be beneficial, since we may have missed break-points at higher FEV, %pred, due to these low break-points. As a future perspective it would also be interesting to see how our data would appear in relation to airway thickness or emphysema grade estimated by computed tomography.

### **Conclusion**

This study has shown that a discontinuous analysis, using three different regression methods, gives new possibilities aside from the standard categorical approach when studying a broad COPD population. In addition, the results give support to the progression of lung destruction, starting in the small airways, followed by diminished gas exchange and hyperinflation, and finally more advanced emphysema. Thereby, our results also support that spirometry preferably should be complemented by methods measuring small airways, RV, diffusion capacity, and reactance. The number of identified break-points in the middle of GOLD Stage II may have important clinical and scientific implications.

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### **Author contributions**

GE initiated this "post-hoc" study, interpreted the data, and wrote the paper. LJ designed the study, tested the patients and interpreted data, and wrote the paper. SP proposed and performed advanced statistical analysis, interpreted the data and revised the paper critically. JA included patients and revised the paper critically. LB designed the study, interpreted data, and revised the paper critically. ET designed the study, interpreted data, and revised the paper critically. All authors contributed toward data analysis, drafting and critically revising the paper and agree to be accountable for all aspects of the work.

### **Disclosure**

The authors report no conflicts of interest in this work.

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